

# Multi-Cluster, Mixed-Mode Computational Modeling of Human Head Conductivity

**Adnan Salman**<sup>1</sup>, Sergei Turovets<sup>1</sup>, Allen Malony<sup>1</sup>,  
and Vasily Volkov

<sup>1</sup> NeuroInformatics Center, University of Oregon

<sup>2</sup> Institute of Mathematics, Minsk, Belarus

# Collaboration

- NeuroInformatics Center, University of Oregon:
  - Robert Frank
- Electrical Geodesic, Inc :
  - Peter Lovely, Colin Davey, Pieter Poolman, Jeff Eriksen ,  
and Don Tucker

# Motivation

- Goal: To estimate the electrical conductivities of human head based on realistic segmented MRI or CT scans

## Necessary for ...

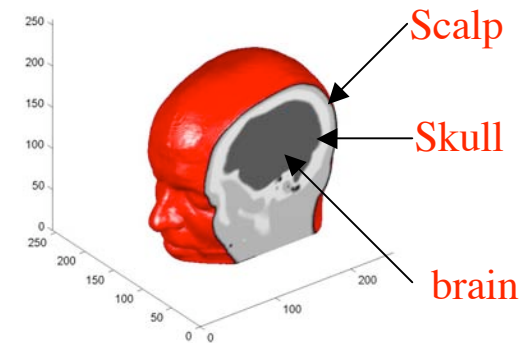
- Source Localization: find the electrical source generator for the potential that can be measured at the scalp
- Detecting abnormalities: cracks, holes, ... etc

# Building Computational Head Models

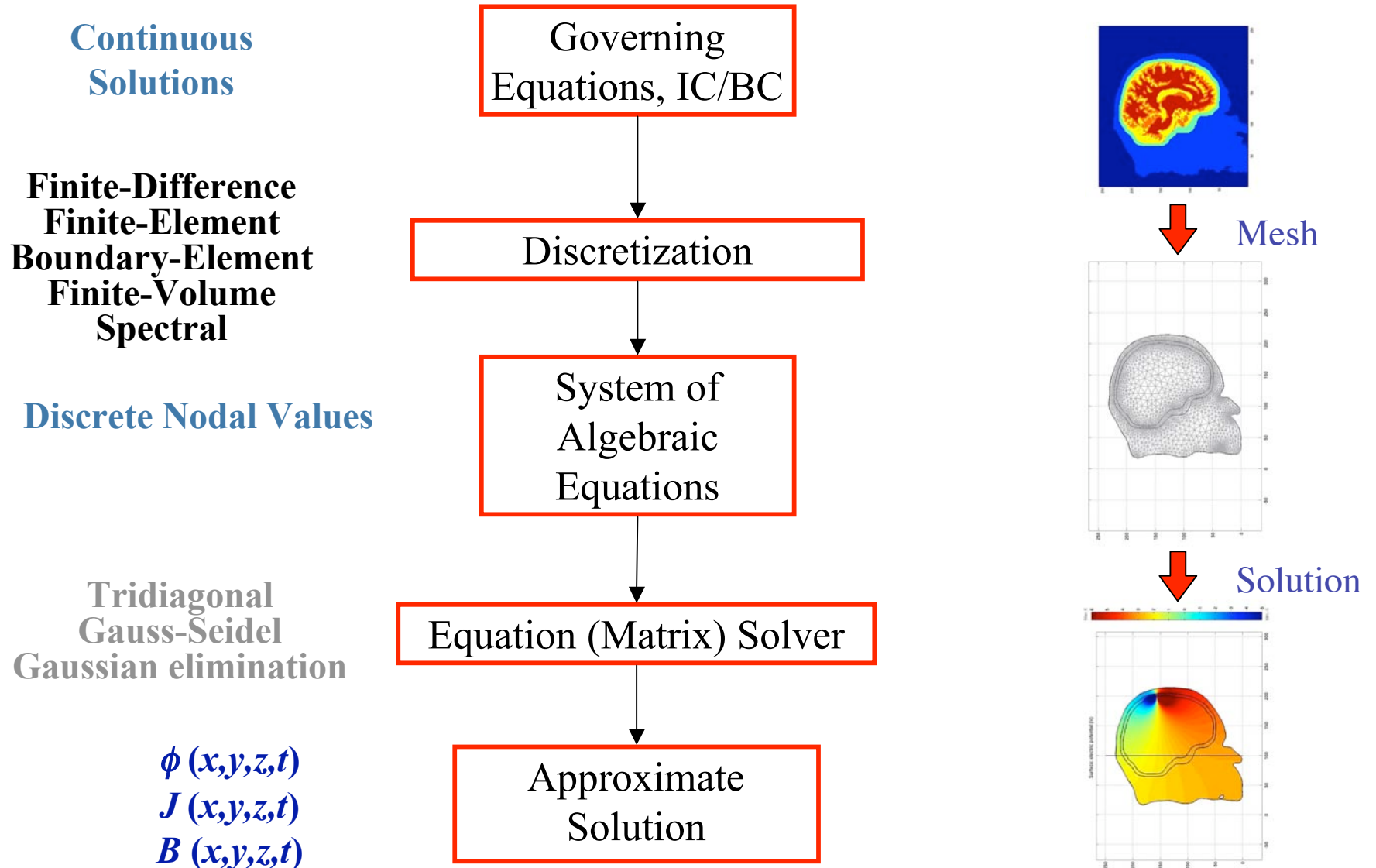
To relate the neural activity in the head to the EEG measurements on the scalp

- Three parts in constructing a human head model
  1. **Geometry:** Geometrical Model of the head with its tissue types
    - Sphere models: 4-sphere model, 3-sphere model
    - MRI or CT: determines the boundaries of the major head tissues
  2. **Electrical Conductivity model:** Assign a conductivity value for each tissue type
    - Homogenous: Assign an average value for the entire MRI segment
    - Known: For each tissue type it varies considerably
  3. **Forward problem:** Evolution of the potential within each tissue.

Given the conductivities of the head tissue and the current sources, find the potential at each point in the head.



# Computational Head Models: Forward problem



# Computational Head Models: Forward problem

The governing equation is:

- The Poisson equation

$$\nabla \cdot (\sigma \nabla \phi) = \nabla \cdot J^s, \quad \text{in } \Omega$$

- With the boundary condition

$$\sigma(\nabla \phi) \cdot n = 0, \quad \text{on } \Gamma_{\Omega}.$$

Where,  $\sigma = \sigma_{ij}(x, y, z)$  is a tensor of the head tissues conductivity,  $J^s$ , current source.

# Computational Head Models: Forward problem

## Multi-component ADI Method:

- unconditionally stable in 3D
- accurate to  $O(\tau + \Delta x^2 + \Delta y^2 + \Delta z^2)$

$$\frac{\phi_i^{n+1} - \overline{\phi^n}}{\tau} + \delta_x \phi_i^{n+1} + \delta_y \phi_j^n + \delta_z \phi_k^n = S$$

$$\frac{\phi_j^{n+1} - \overline{\phi^n}}{\tau} + \delta_x \phi_i^{n+1} + \delta_y \phi_j^{n+1} + \delta_z \phi_k^n = S$$

$$\frac{\phi_k^{n+1} - \overline{\phi^n}}{\tau} + \delta_x \phi_i^{n+1} + \delta_y \phi_j^{n+1} + \delta_z \phi_k^{n+1} = S$$

Here :  $\overline{\phi^n} = (\phi_i^n + \phi_j^n + \phi_k^n) / 3$

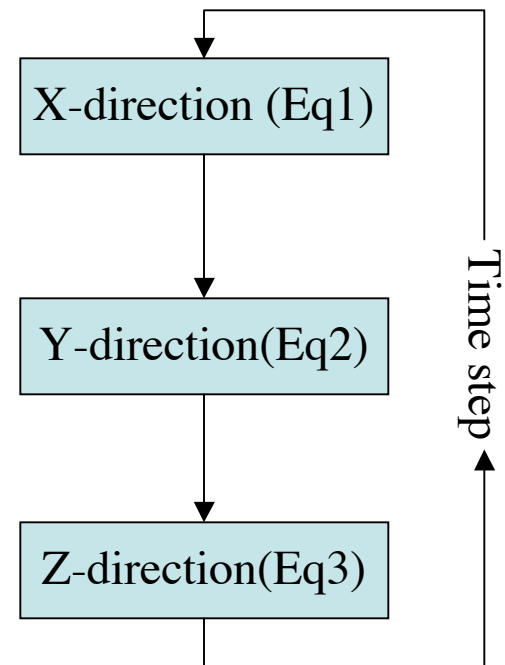
$\delta_{x,y,z}$  is notation for an 1D second order spatial difference operator

Reference: [Abrashin et al, Differential Equations 37 \(2001\) 867](#)

# Computational Head Models: Forward problem

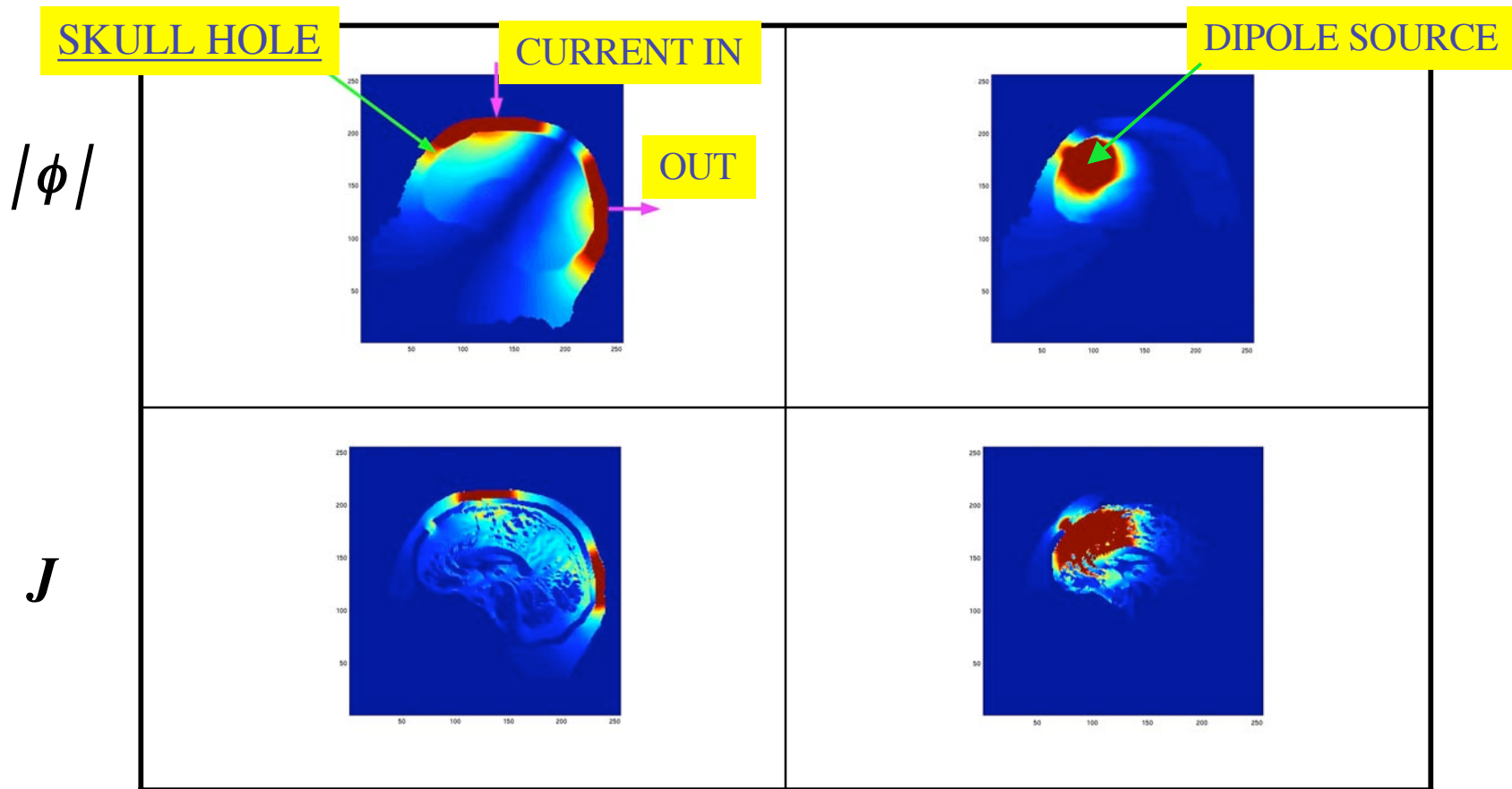
## Multi-component ADI algorithm:

- Each time step is split into 3 substeps
- In each substep we solve a 1D tridiagonal systems





# Computational Head Models: Forward problem: solution

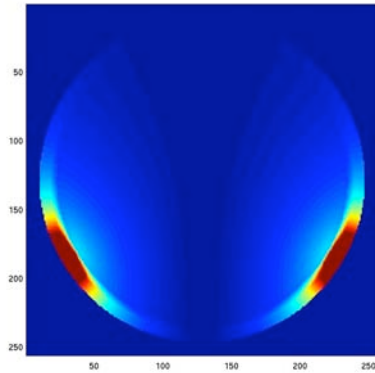


External Current Injection  
(Electrical Impedance Tomography)

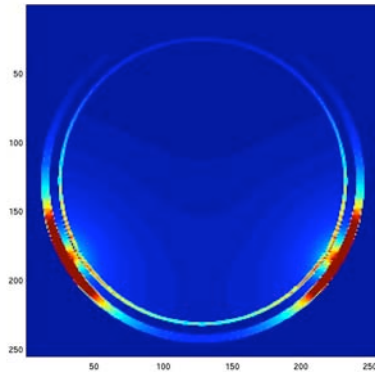
Intracranial Dipole Source Field  
(Epileptic Source Localization)

# Computational Head Models: Forward problem: Validation

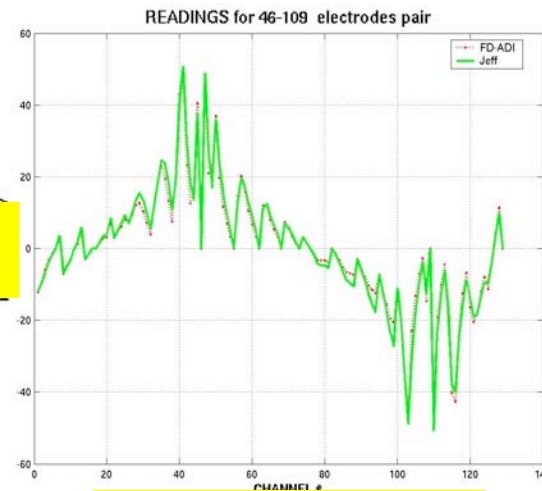
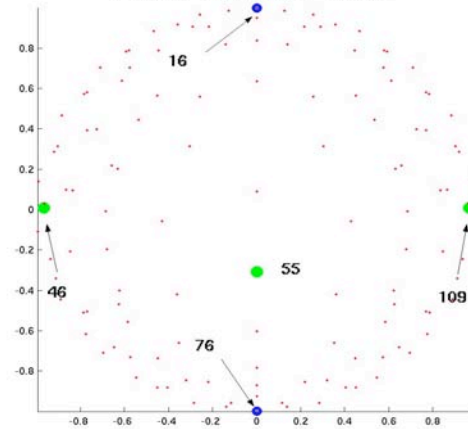
$|\phi|$



$J$



Electrode Montage: XY view



Electrode Number

# Computational Head Models: Forward problem: Parallelization

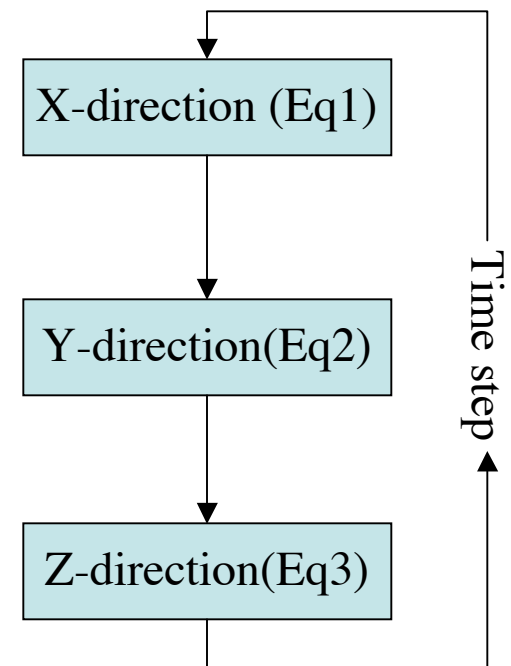
- The computation to solve the system of equations in each substep is independent of each other
- Example: in the x direction we can solve the  $N_y N_z$  equations concurrently on different processors
- The Parallel program structure is:

For each time step

- Solve  $N_y N_z$  tridiagonal equations
- Solve  $N_x N_y$  tridiagonal equations
- Solve  $N_y N_z$  tridiagonal equations

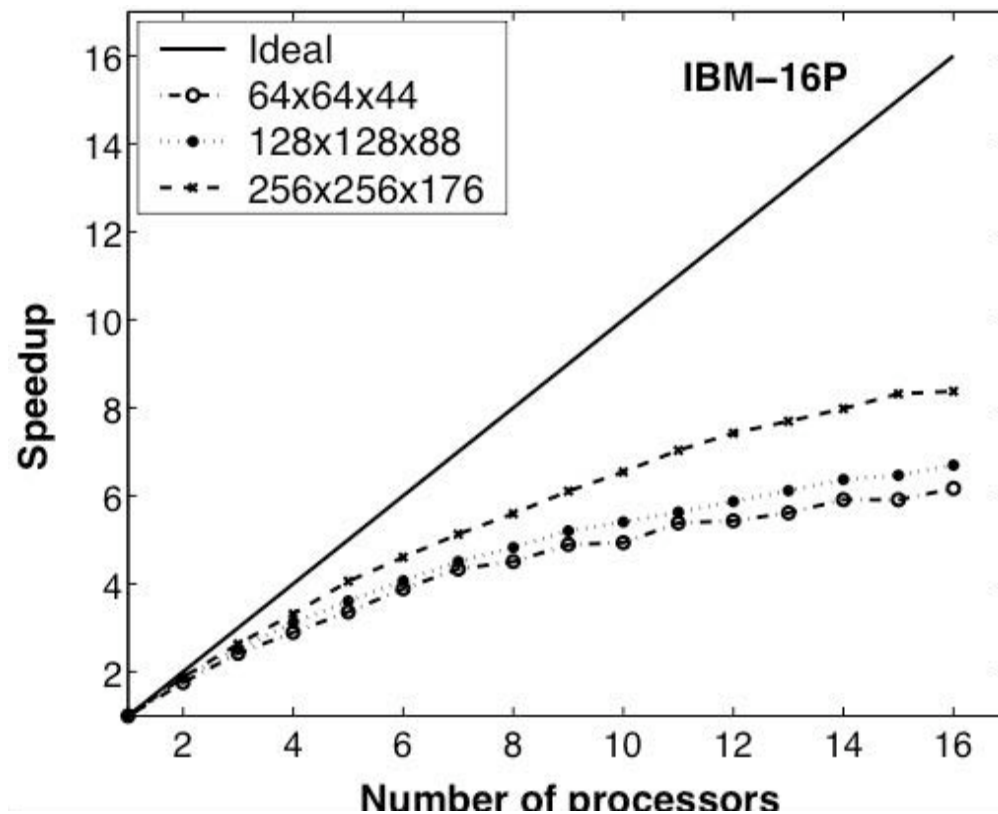
End

- We used openMP to implement the parallel code in a shared memory clusters



# Computational Head Models: Forward problem: Parallelization speedup

Forward Solution Speedup on IBM-P690



# Computational Head Models: Inverse Problem

- Given the measured electric potential at the scalp  $V_i$ , the current sources and the head tissue geometry

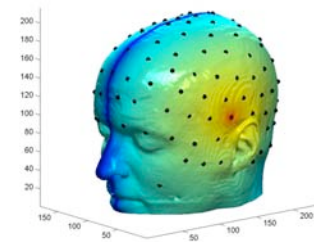
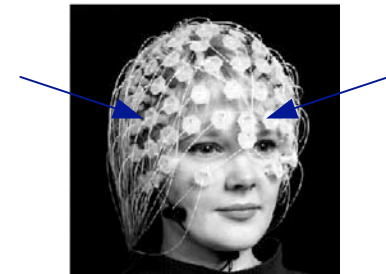
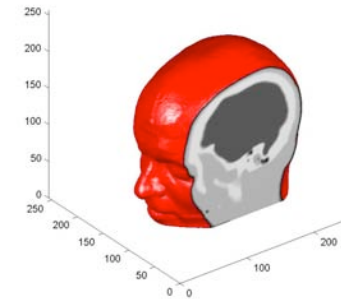
Estimate the conductivities of the head tissues

The procedure to estimate the tissue conductivities is:

- Small currents are injected between electrode pairs
- Resulting potential measured at remaining electrodes
- Find the conductivities that produce the best fit to measurements by minimizing the cost function:

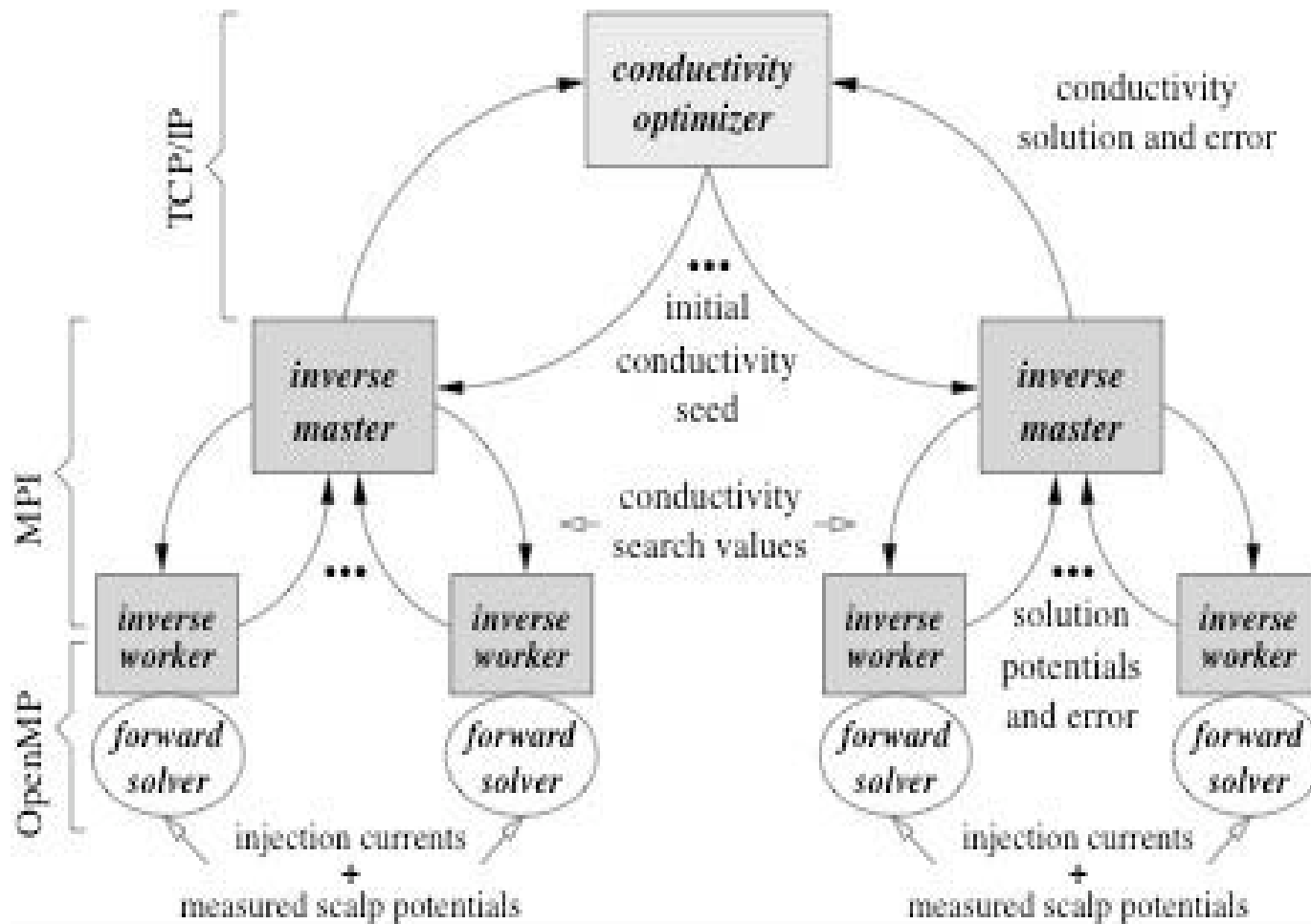
$$E = \left[ \frac{1}{N} \sum_{i=1}^N (\phi_i^p - V_i)^2 \right]^{1/2}$$

- Computationally intensive



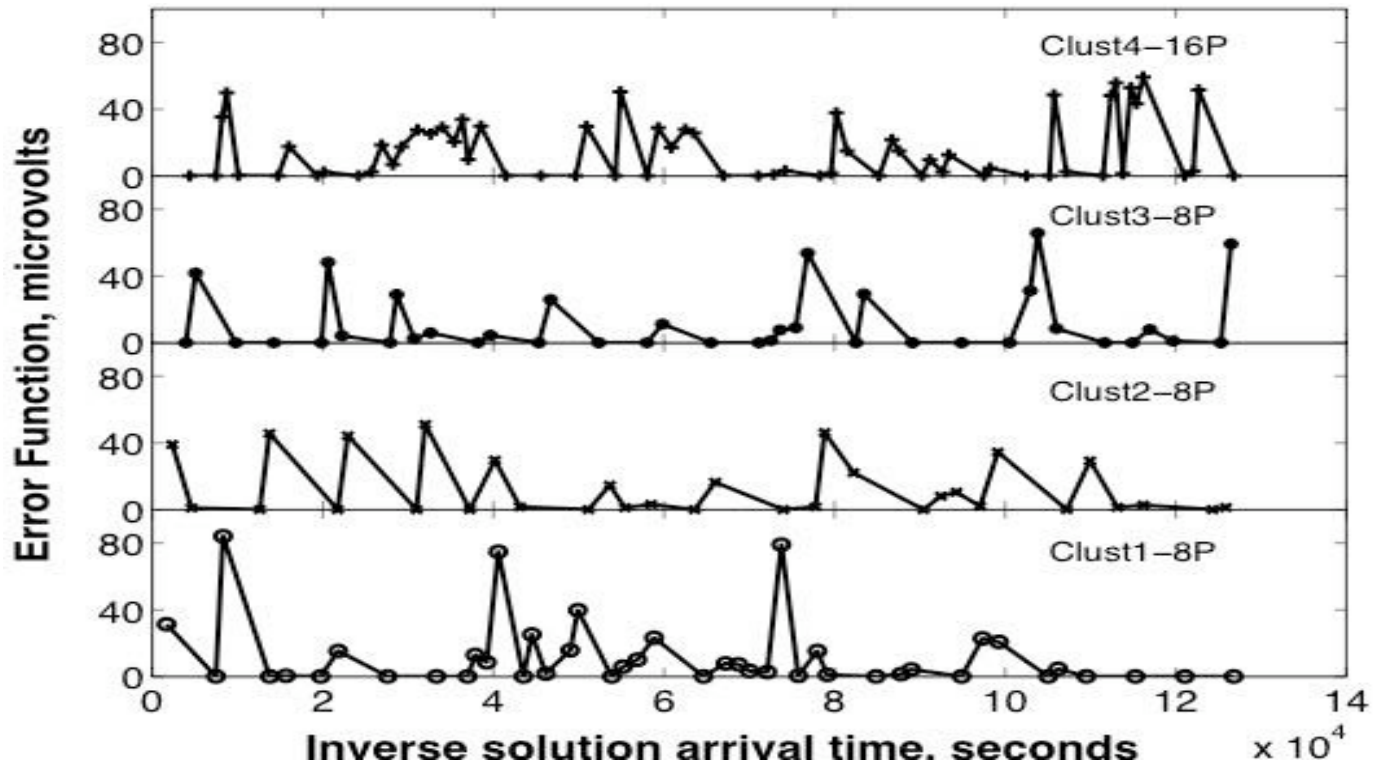
Computational model

# Schematic view of the parallel computational system



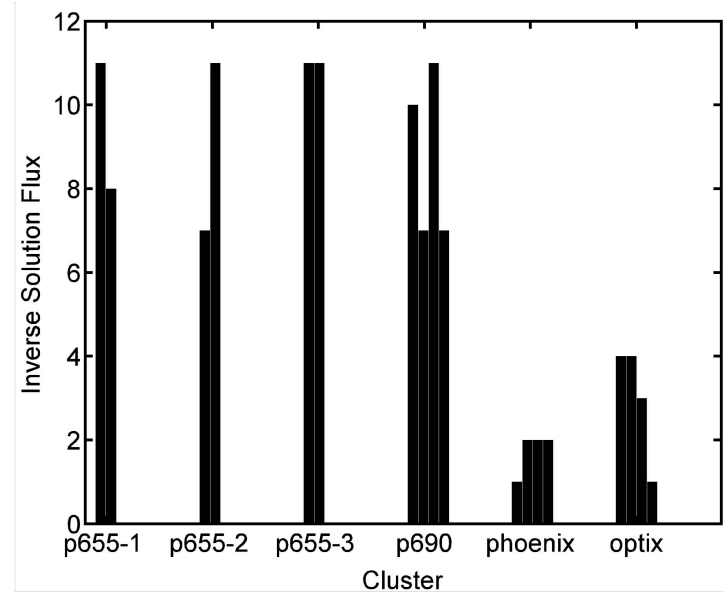
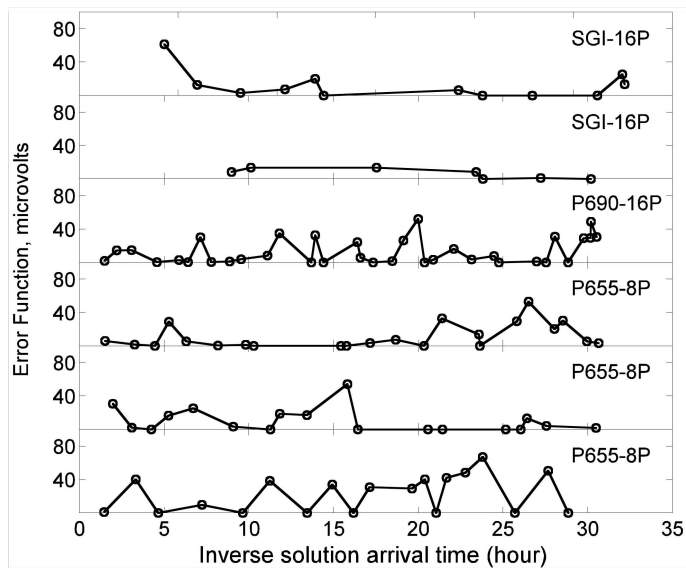
# Performance Statistics

## Dynamics of Inverse Search



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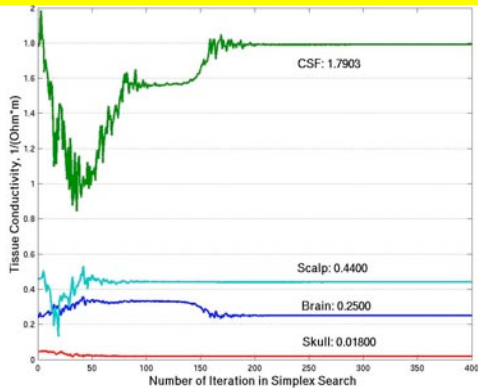




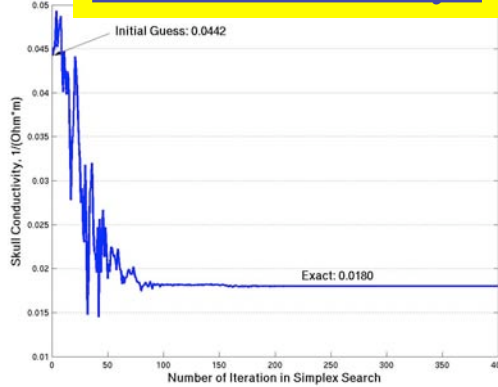
# Inverse Problem: Simplex Algorithm

simulated data (real MRI)

## Dynamics of Inverse Solution:



## Skull Conductivity :



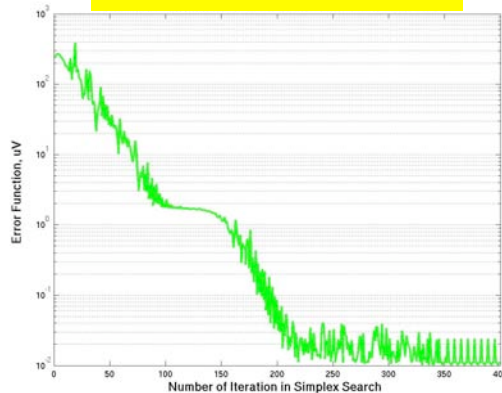
## Error Function to minimize:

$$E = \left[ \frac{1}{N} \sum_{i=1}^N (\phi_i^p - V_i)^2 \right]^{1/2}$$

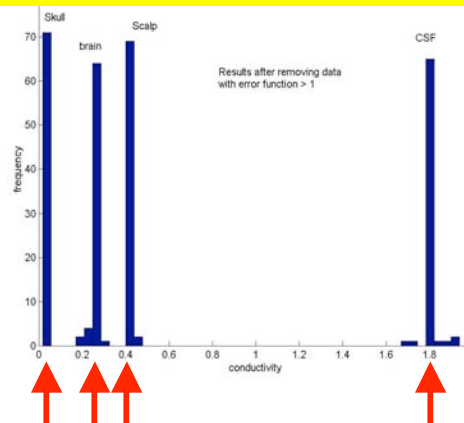
## Retrieved tissues conductivities

Tissue type	$\sigma(\Omega^{-1}\text{m}^{-1})$	$\Delta\sigma(\Omega^{-1}\text{m}^{-1})$
Brain	0.2491	0.0099
CSF	1.7933	0.0311
Skull	0.0180	0.00017
Scalp	0.4400	0.00024

## Error Dynamics:



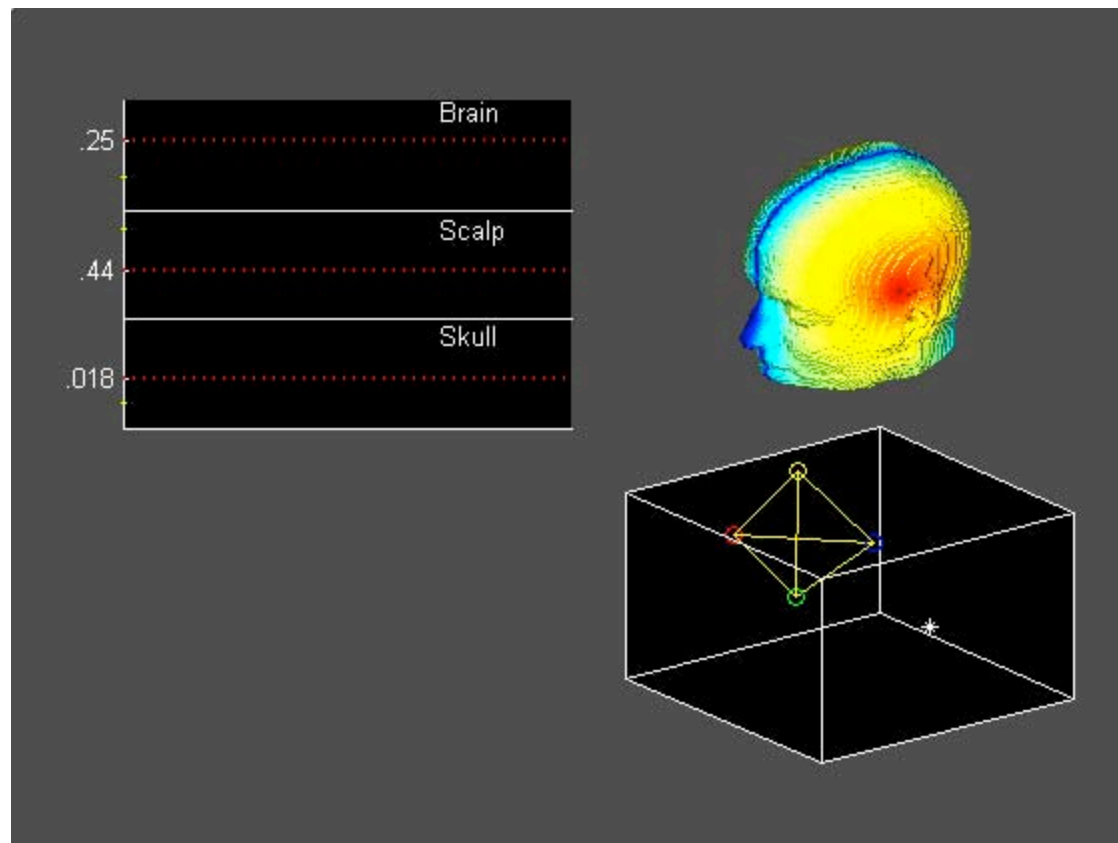
## Extracted Conductivities



Exact Values

# Inverse Problem: Simplex Algorithm

simulated data (real MRI)



# Summary

- Finite Difference ADI algorithm based 3D solvers for the forward electrical have been developed and tested for variety of geometries;
- The electrical forward solver has been optimized and parallelized within OpenMP protocol of multi-threaded, shared memory parallelism to run on different clusters;
- The successful demonstrations of solving the nonlinear inverse problem with use of HPC for search and estimation of the unknown head tissues conductivity have been made for 4-tissues segmentation on the realistic MRI based geometry ( $128^3$  resolution) of the human head;
- The work with experimental human data is in progress

Thank you ....

Questions

